

Summary

Problem statement

- EEG data is noisy and variable across subjects, making it difficult to extract generalizable signals¹.
- A key aim in EEG analysis is to extract the underlying neural activation (content) while accounting for individual subject variability (style).
- We hypothesize that the auxiliary task of optimizing EEG signal conversion between tasks and subjects requires the learning of latent representations explicitly accounting for content and style.

Method

- A novel contrastive split-latent permutation autoencoder (CSLP-AE) framework is proposed that directly optimizes for EEG conversion.
- The split-latent representations are guided using contrastive learning to promote the latent splits to explicitly represent subject and task.

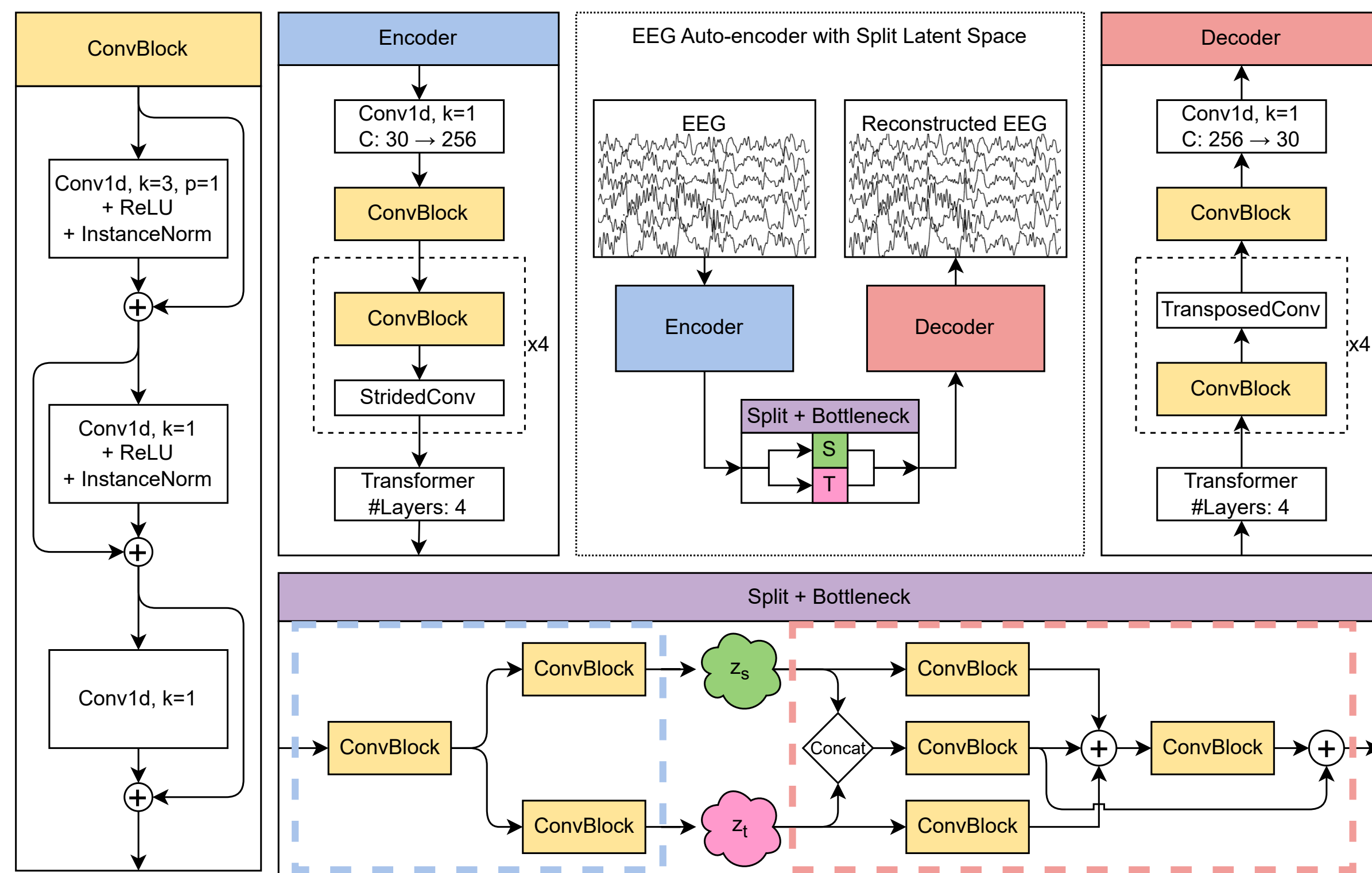
Main conclusions

- CSLP-AE provides favourable generalizable subject and task characterizations compared to supervised, unsupervised and self-supervised (contrastive) learning frameworks.
- The procedure also enables zero-shot conversion between unseen subjects.
- The proposed CSLP-AE provides a general framework for signal conversion and extraction of content (task activation) and style (subject variability) components.

CSLP-AE model architecture

CNN/Transformer-based autoencoder with split latent space:

- Latent space split into subject (z^s) and task (z^T) spaces.
- Consists of ConvBlocks and a Transformer bottleneck.



Dual-component loss objective balancing reconstruction and contrastive learning

$$L(\mathbf{X}, \mathbf{Z}) = [L_{LP}(\mathcal{T}; \mathbf{X}^a, \mathbf{X}^b) + L_{LP}(\mathcal{S}; \mathbf{X}^a, \mathbf{X}^b)] + \alpha [L_{CLIP}(\mathbf{Z}^{(s,a)}, \mathbf{Z}^{(s,b)}) + L_{CLIP}(\mathbf{Z}^{(T,a)}, \mathbf{Z}^{(T,b)})]$$

- MSE-based latent permutation loss for both subject (s) and task (T) permutation.

$$L_{LP}(\mathcal{L}; \mathbf{X}^a, \mathbf{X}^b) = \frac{1}{N} \sum_{j=1}^N (\|\mathbf{x}_j^a - \hat{\mathbf{x}}_j^{(L,a)}\|_2^2 + \|\mathbf{x}_j^b - \hat{\mathbf{x}}_j^{(L,b)}\|_2^2)$$

- Contrastive learning using multi-class N-pair temperature-scaled symmetrical cross-entropy loss.

$$L_{NT-Xent}(\mathbf{Z}^i, \mathbf{Z}^{j'}) = -\log \frac{\exp(\text{sim}(\mathbf{z}_k^i, \mathbf{z}_k^{j'})/\tau)}{\sum_{i=1}^K \sum_{j=1}^K \mathbb{1}_{[i \neq j]} \exp(\text{sim}(\mathbf{z}_k^i, \mathbf{z}_k^{j'})/\tau)}$$

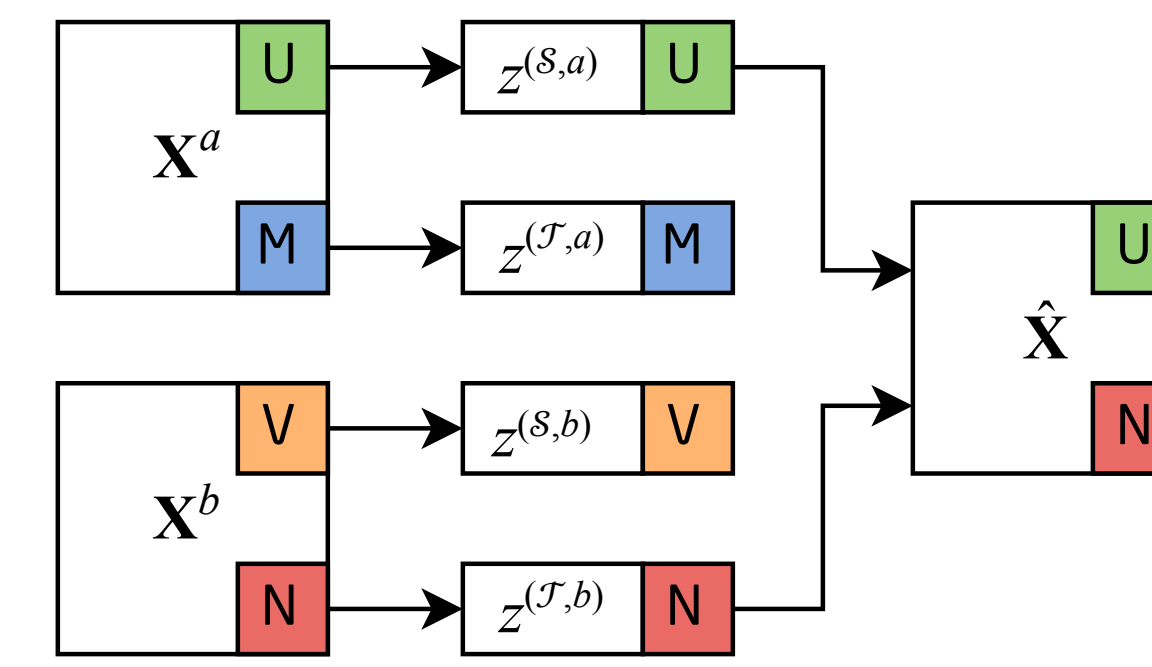
$$L_{CLIP}(\mathbf{Z}^A, \mathbf{Z}^B) = \frac{1}{K} \sum_k (L_{NT-Xent}(\mathbf{Z}^A, \mathbf{Z}^B, k) + L_{NT-Xent}(\mathbf{Z}^B, \mathbf{Z}^A, k))$$

- Parameter α controls the trade-off between optimizing for conversion or specialization of the latent space. Here, we focus on the case of $\alpha = 0$ (pure permutation loss, SLP-AE) and $\alpha = 1$ (equal contribution).

EEG conversion

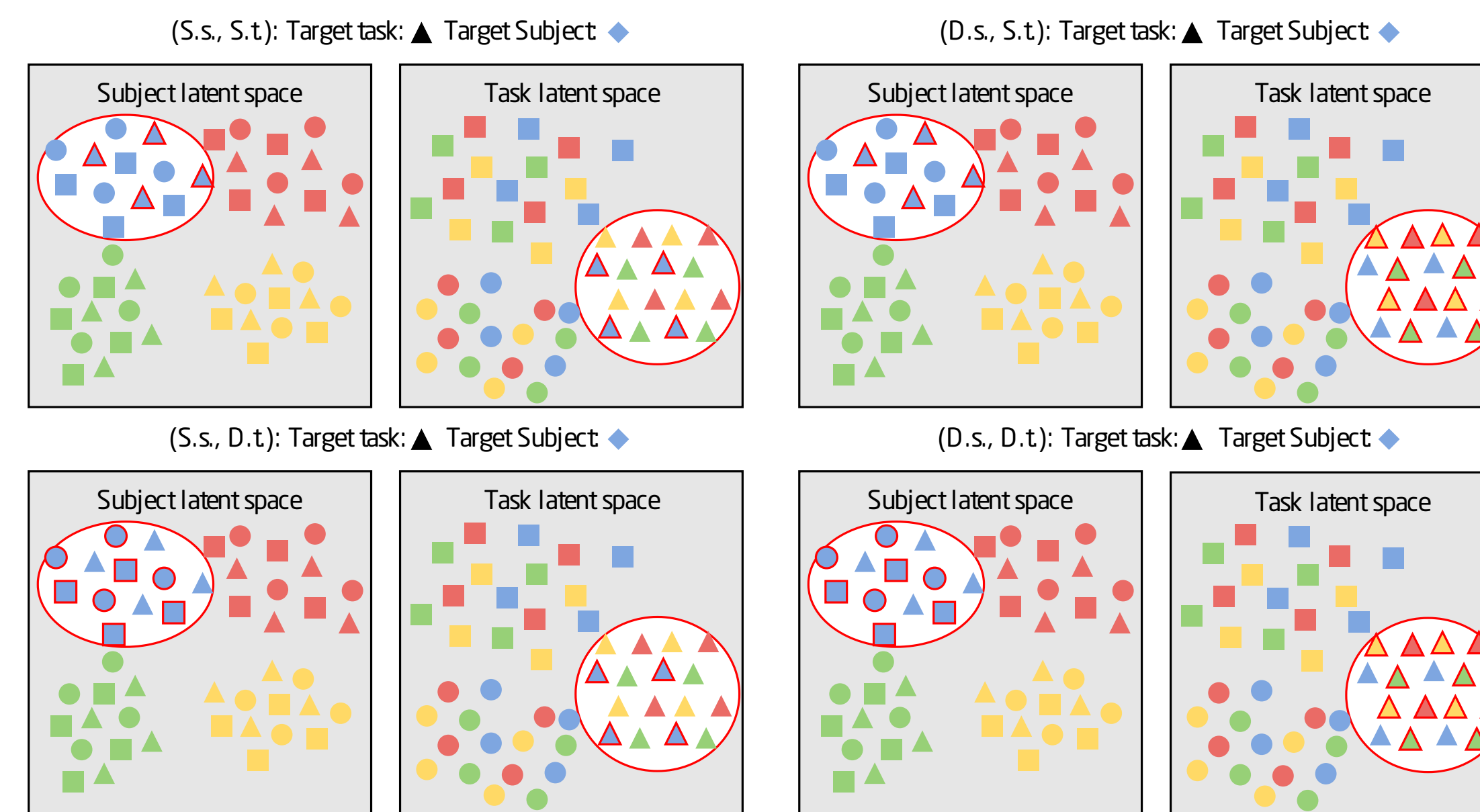
Ideal conversion

- Latent representations contain specialized information about subjects and tasks. Conversion is possible by switching respective latents from samples a and b .
- A successful conversion (illustrated for task conversion) is decoded from subject latent U and task latent N yielding a converted signal \hat{X} representing subject U performing task N .



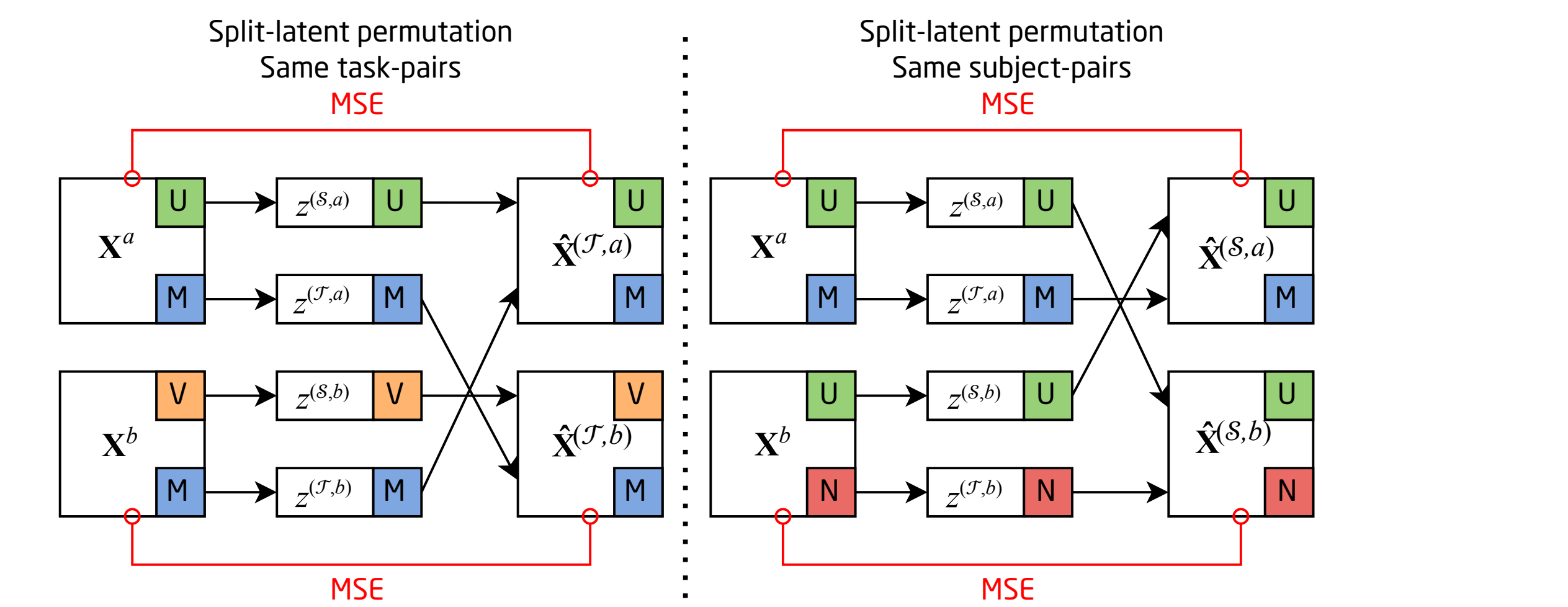
Conversion schemes

- We define four conversion schemes denoting which latent representations are used for the conversion.
 - S.s. and D.s. denote same and different subject, respectively.
 - S.t. and D.t. denote same and different task, respectively.
 - Subjects are shown as colors and tasks are shown as shapes.



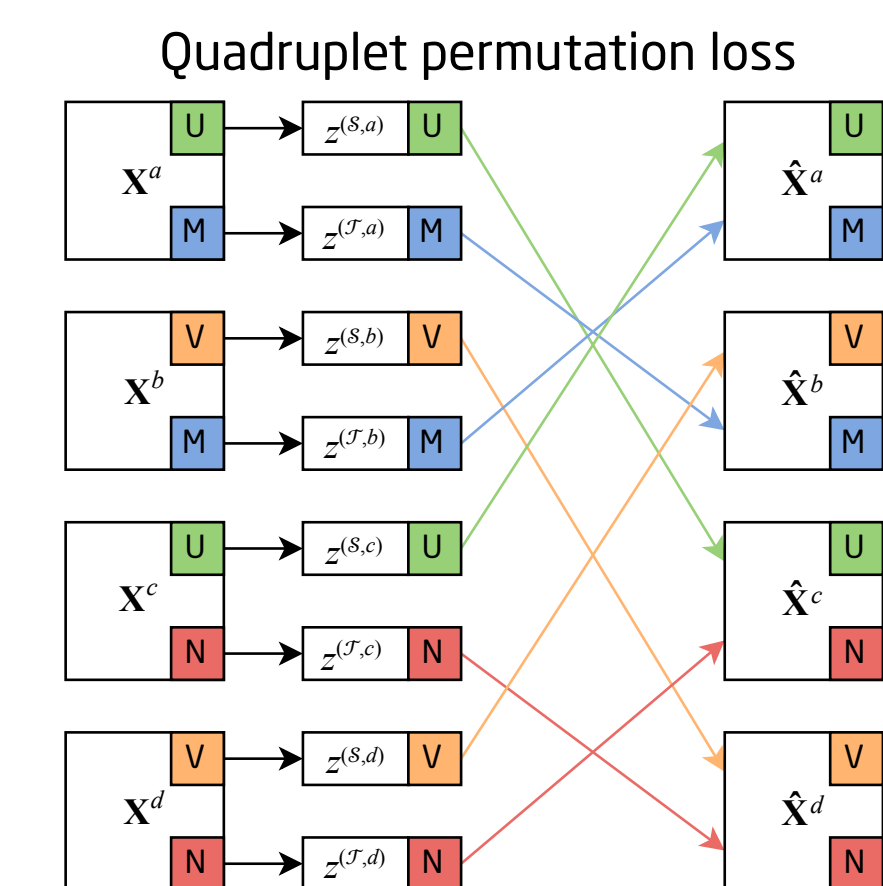
Split-latent permutation

- Sampling is performed such that each batch contains a pair of samples for each subject and for each task.
- For same-task pairs the task latent representations are swapped during training, while for same-subject pairs the subject latent representations are swapped.



Quadruplet permutation

- The batch is sampled to contain four samples each with a combination of tasks M and N and subjects U and V .
- No direct pathway from conversion (output) to sample (input).
- Quadruplet loss consists of four terms for each latent space.



$$L_{QP}(\mathcal{L}; \mathbf{X}^a, \mathbf{X}^b, \mathbf{X}^c, \mathbf{X}^d) = \frac{1}{4N} \sum_{j=1}^N (\|\mathbf{x}_j^a - \hat{\mathbf{x}}_j^{(L,a)}\|_2^2 + \|\mathbf{x}_j^b - \hat{\mathbf{x}}_j^{(L,b)}\|_2^2 + \|\mathbf{x}_j^c - \hat{\mathbf{x}}_j^{(L,c)}\|_2^2 + \|\mathbf{x}_j^d - \hat{\mathbf{x}}_j^{(L,d)}\|_2^2)$$

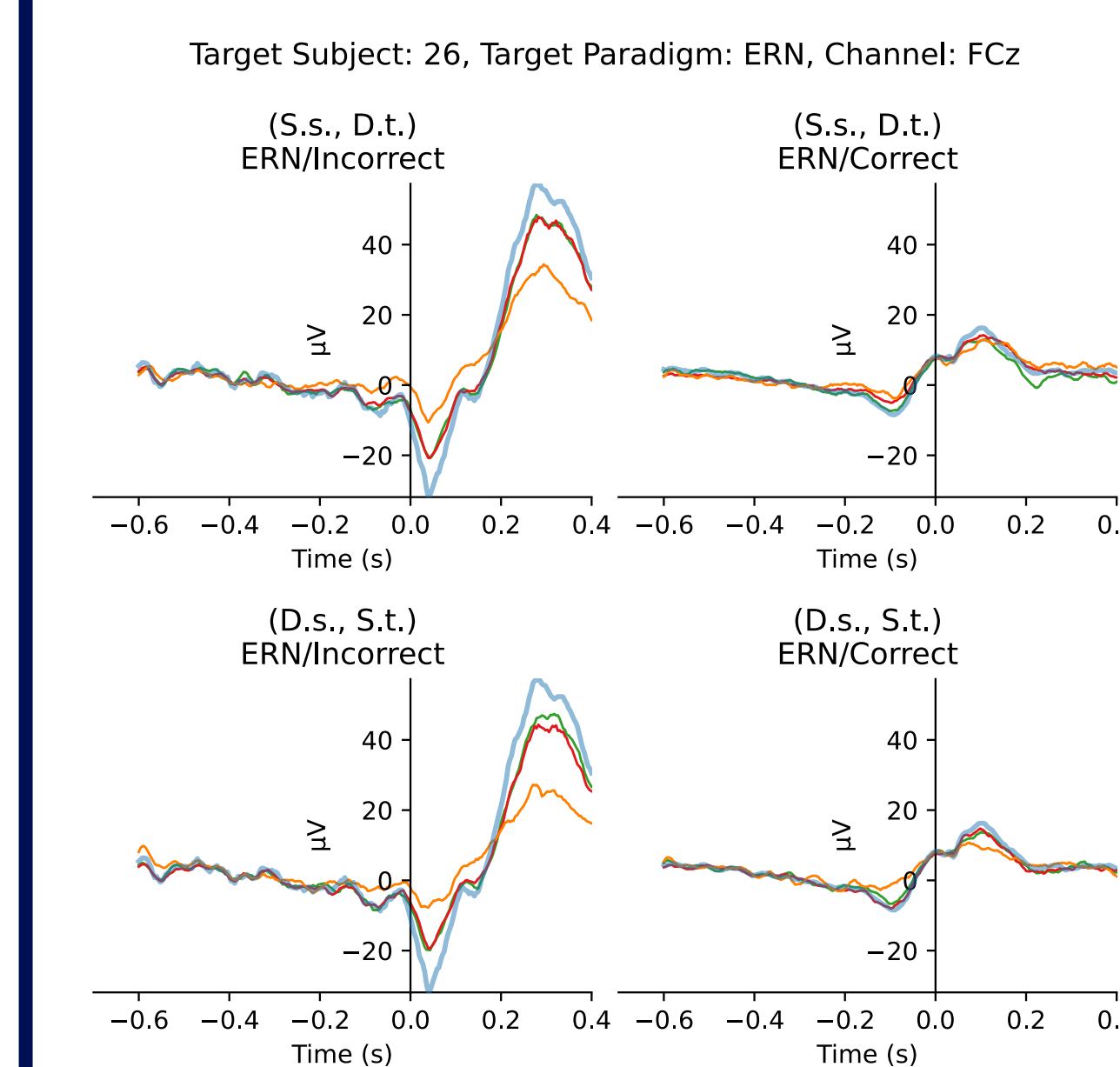
Experimental results

Superior performance in EEG analysis on unseen subjects

- High classification accuracies in both subject and task classification from EEG data.
- Effective zero-shot EEG conversion across various scenarios.
- Quadruplet permutation without contrastive learning obtains highest task classification accuracy and (D.s., D.t.) conversion.

| Model | S.acc% | Ti-S.acc% | T.acc% | S-T.acc% | (S.s.,S.t.) | (D.s.,D.t.) | (D.s.,S.t.) | (S.s.,D.t.) |
|---------|-------------------|------------|-------------------|------------|------------------|------------------|------------------|------------------|
| CSLP-AE | 76.10±0.76 | 43.36±0.46 | 46.17±0.25 | 76.47±0.46 | 1.91±0.08 | 6.90±0.05 | 3.43±0.05 | 3.94±0.16 |
| SQP-AE | 69.26±0.50 | 46.86±1.35 | 44.80±0.77 | 69.60±0.25 | 1.48±0.05 | 6.44±0.03 | 2.87±0.10 | 2.97±0.05 |
| SQP-AE | 73.04±0.50 | 35.89±0.42 | 44.83±0.21 | 71.56±0.64 | 6.20±0.12 | 7.00±0.08 | 6.60±0.11 | 6.59±0.10 |
| SQP-AE | 73.44±0.33 | 43.92±0.29 | 48.88±0.13 | 70.42±0.39 | 5.58±0.07 | 6.49±0.04 | 6.07±0.04 | 5.99±0.06 |
| CSLP-AE | 80.32±0.28 | 45.41±0.37 | 48.48±0.34 | 79.64±0.37 | 4.21±0.12 | 20.06±0.10 | 5.80±0.15 | 6.65±0.23 |
| SLP-AE | 74.63±0.74 | 47.23±0.31 | 47.00±0.32 | 74.70±0.73 | 3.82±0.04 | 19.92±0.10 | 6.12±0.09 | 5.02±0.08 |
| C-AE | 79.42±0.48 | 37.34±0.45 | 46.59±0.23 | 73.27±0.25 | 4.28±0.06 | 20.28±0.07 | 11.33±0.47 | 10.64±0.30 |
| AE | 60.68±0.16 | 31.62±0.27 | 31.43±0.28 | 61.08±0.38 | 3.54±0.12 | 20.82±0.07 | 11.20±0.32 | 10.74±0.48 |
| CL | 78.82±0.46 | 37.65±0.54 | 45.36±0.37 | 71.70±0.55 | - | - | - | - |
| CE | 79.25±0.37 | 35.52±0.38 | 45.22±0.23 | 64.73±0.44 | - | - | - | - |
| CE(t) | - | - | 45.80±0.24 | 44.27±0.59 | - | - | - | - |
| CSP | - | - | 35.22±0.11 | 69.89±0.10 | - | - | - | - |

Generalizable EEG conversion for unseen subjects

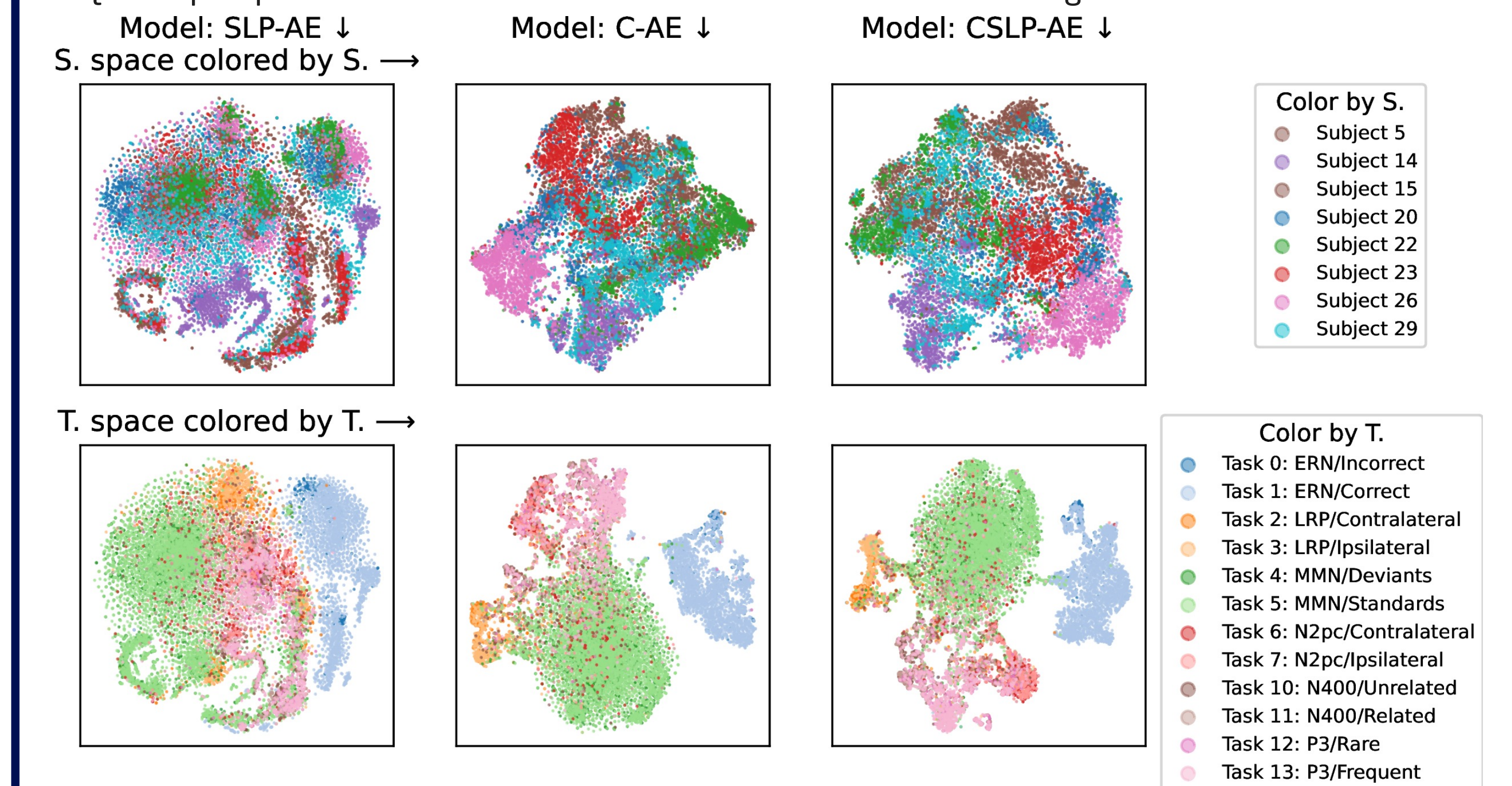


Competitive out-of-domain performance with only slight degradation in continuous domains

| Model | EEGMMI | SleepEDFx |
|--|------------|------------|
| CSLP-AE (this work) | 64.28±0.16 | 75.16±0.95 |
| C-AE (this work) | 61.89±0.41 | 75.16±0.86 |
| SLP-AE (this work) | 57.93±0.56 | 70.59±1.18 |
| EEGNet (Wang et al. ²) | 65.07 | - |
| f-Ctrans (Xie et al. ³) | 64.22 | - |
| CNN (Dose et al. ⁴) | 58.59 | - |
| XSleepNet2 (Phan et al. ⁵) | - | 84 |
| Zhu et al. ⁶ | - | 82.8 |
| SeqSleepNet (Phan et al. ⁷) | - | 82.6 |
| SleepTransformer (Phan et al. ⁸) | - | 81.4 |
| AttnSleep (Eidele et al. ⁹) | - | 81.3 |
| SleepEEGNet (Mousavi et al. ¹⁰) | - | 80 |

Contrastive learning is required for specialized latent spaces

- Structural encoding in duplicated latent spaces.
- Quadruplet permutation loss is an alternative to contrastive learning.



References: 2. Wang et al., *IEEE MeMeA*, 2020. 3. Xie et al., *IEEE Trans. Neural Syst. Rehabil. Eng.*, 2022. 4. Dose et al., *Expert Syst. Appl.*, 2018. 5. Phan et al., *IEEE Trans. Pattern Anal. Mach. Intell.*, 2022. 6. Zhu et al., *Int. J. Environ. Res. Public Health*, 2020. 7. Phan et al., *IEEE Trans. Neural Syst. Rehabil. Eng.*, 2019. 8. Phan et al., *IEEE Trans. Biomed. Eng.*, 2022. 9. Eidele et al., *IEEE Trans. Neural Syst. Rehabil. Eng.*, 2021. 10. Mousavi et al., *PLoS One*, 2019.

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